# Time-Harmonic Optical Flow with Applications in Elastography

Oleh Melnyk<sup>\*†</sup>

Michael Quellmalz<sup>†</sup>

melnyk@math.tu-berlin.de

quellmalz@math.tu-berlin.de

Gabriele Steidl<sup>†</sup>

steidl@math.tu-berlin.de

Noah Jaitner<sup>‡</sup>

noah.jaitner@charite.de

Jakob Jordan<sup>‡</sup>

jakob.jordan@charite.de

ingolf.sack@charite.de

Ingolf Sack<sup>‡</sup>

In this paper, we propose mathematical models for reconstructing the optical flow in time-harmonic elastography. In this image acquisition technique, the object undergoes a special time-harmonic oscillation with known frequency so that only the spatially varying amplitude of the velocity field has to be determined. This allows for a simpler multi-frame optical flow analysis using Fourier analytic tools in time. We propose three variational optical flow models and show how their minimization can be tackled via Fourier transform in time. Numerical examples with synthetic as well as real-world data demonstrate the benefits of our approach.

*Keywords:* optical flow, elastography, Fourier transform, iteratively reweighted least squares, Horn–Schunck method

### 1. Introduction

The tracking of motion along the sequence of image frames is a prominent problem in computer vision. The main goal consists in finding the motion vector field between image frames of moving or deformed objects. Optical flow methods trace back to the works of Horn–Schunck [15] and Lucas–Kanade [21]. The former is an instance of variational methods, which have proven to be a powerful tool for this task. The idea is to minimize a

<sup>\*</sup>Corresponding author.

<sup>&</sup>lt;sup>†</sup>Technische Universität Berlin, Institute of Mathematics, Straße des 17. Juni 136, D-10623 Berlin, Germany

<sup>&</sup>lt;sup>‡</sup>Charité Universitätsmedizin Berlin, Department of Radiology, Charitéplatz 1, D-10117 Berlin, Germany

Tikhonov-type energy functional consisting of data fidelity and smoothness terms. For an overview, we refer to the review papers [6, 11, 45] as well as the performance comparisons [4], and the more recent meta performance analysis [48]. Practical implementations of the optical flow estimation further rely on a combination of heuristics such as a coarse-to-fine pyramid, image warping, and inertial smoothing between iterations as highlighted in the extensive experimental evaluations in [37, 38]. Finally, neural network-based methods such as RAFT [39] and its multi-frame variants [43] or Videoflow [36] have shown state-of-the-art solutions for generalized optimal flow problems. Motion magnification based on RAFT was also studied in [10]. An excellent overview of neural network-based solutions is presented in [16]. A review comparing learning-based and model-based strategies is given in [33].

An important application of optical flow methods lies in image modalities of quantitative elastography, where one estimates the parameters of elastic deformation, see [29, 31], in particular for OCT (optical coherence tomography) elastography [18, 32] and ultrasound elastography [40]. In this context, specific challenges come in due to speckles caused by interference of scattered waves [35] and also the need to extend optical flow models by incorporating boundary conditions [34].

Time-harmonic elastography was originally applied in magnetic resonance imaging (MRI). In MRI elastography, shear wave fields are successively encoded in synchrony with the repeated acquisition of lines or segments of image space [31]. Although initially proposed as a way to overcome the time limitations of relatively slow MRI acquisitions, it has become clear that time-harmonic shear waves possess three compelling advantages over transient waves: first, they efficiently deliver shear energy to deeper tissue layers; second, they allow the drive frequency to be adapted to the field of view; and finally, they allow the shear modulus to be interrogated at a precisely known excitation frequency, facilitating direct comparison of values across the length scales addressed by different elastography techniques [24]. Consequently, time-harmonic shear waves have been used in ultrasonic elastography [42] and, more recently, in optical elastography [49].

In this paper, we consider a special optical flow problem for multiple image frames arising from optical time-harmonic elastography [17]. More precisely, an external acoustic source, whose frequency is precisely controlled by a wave generator, causes a timeharmonic oscillation of the specimen. Here, we assume that the flow velocity has the special structure  $v(t, x) = \operatorname{Re}(a(x)e^{i\omega t}) \in \mathbb{R}^d$ , which consists of a harmonic wave in time  $t \ge 0$  with known frequency  $\omega$  and an amplitude a(x) depending only on the spatial variable  $x \in \mathbb{R}^d$ . Having reconstructed the velocity field v, it can be used in a subsequent step e.g. for the analysis of the material properties considered in the time-harmonic elastography experiment. In particular, it is possible to reconstruct the shear modulus of the considered material which is an important property that characterizes the mechanical behavior of the material, see [31].

Given a sequence of images of the specimen undergoing a harmonic deformation over multiple time steps t, we have only to reconstruct the time-independent amplitude a to get access to the displacement. Therefore, we can efficiently utilize the image frames over the whole time period, i.e., a multiframe approach for reconstructing the velocity field. In contrast, most variational methods for general optical flow reconstruction rely just on two (consecutive) image frames. Nevertheless, there exist a few variational multiframe approaches, one of the first ones was that of Schnörr and Weickert [46]. Furthermore, a periodic model, which is not necessarily a single harmonic, was considered in the context of cardiac motion [20] and solved with the Horn–Schunck method. This model was extended in [28] to a smoothed version of the total variation norm and solved via gradient descent. The main advantage of our approach to the existing ones is that we directly incorporate the time-harmonicity into our model. Due to their different nature, our model offers a lower numerical complexity, taking advantage of the sparse representation of the vibrations in the Fourier domain and the fact that we need to reconstruct only a single amplitude image.

In this paper, we propose three models to solve the time-harmonic optical flow problem. The first one is an adaption of the classical Horn–Schunck approach with quadratic data fidelity and smoothness term. We give an explicit characterization of the minimizers of the respective energy functional via the Fourier transform in time. Based on this, we suggest solving it efficiently as a least squares problem. The second model comprises an  $L_1$  data fidelity term, making it more robust to noise, and a total variation smoothness term. The third uses "the best of both worlds" by combining the data term of the second with the smoothness of the first model, therefore yielding a smoother amplitude field as expected from the physical point of view. After reformulating in the Fourier domain, both models are solved with an iteratively reweighted least squares (IRLS) method [19, 23]. The accuracy and the lower arithmetic complexity of our algorithms are validated in numerical experiments with both simulated and experimental data acquired in a gel phantom and a biofilm.

**Outline of the paper.** We start by providing our mathematical optical flow model in time-harmonic elastography in Section 2. Then, in Section 3, we propose three variational models to approximate the optical flow. We derive formulas for finding the minimizing amplitude of the optical flow field using Fourier transforms. Implementation details are discussed in Section 4. Both synthetic and real-world examples which demonstrate the very good numerical performance of our approach are given in Section 5. Final conclusions are drawn in Section 6.

### 2. Time-harmonic optical flow

In this section, we provide the continuous optical flow model for the special setting when the object undergoes a time-harmonic oscillation with known frequency.

Let T > 0 be the observational time and  $\Omega$  be a bounded domain in  $\mathbb{R}^d$ . We are given gray-value images  $I: [0,T] \times \Omega \to \mathbb{R}$  in  $C^1$ , which means that they are continuously differentiable in both time and space. In our applications, we deal with sequences of two-dimensional images, i.e. d = 2 and  $\Omega$  is a rectangular domain. From the experimental setting, we can assume that the so-called "brightness constancy" assumption holds true, meaning that the image gray-values (pixel intensities) move in space, but do not change their values. Roughly speaking, we assume for all  $x \in \Omega$  that

$$I(t,\varphi(t,x)) = I(0,x) \quad \text{for all} \quad t \in [0,T],$$
(1)

where  $\varphi \colon [0,T] \times \Omega \to \mathbb{R}^d$  fulfills for every  $x \in \Omega$  the ordinary differential equation (ODE)

$$\frac{\mathrm{d}}{\mathrm{d}t}\varphi(t,x) = v(t,\varphi(t,x)), \quad t \in [0,T], 
\varphi(0,x) = x,$$
(2)

with a sufficiently smooth velocity field  $v \colon [0,T] \times \Omega \to \mathbb{R}^d$ . Then (1) can be rewritten as

$$0 = \frac{\mathrm{d}}{\mathrm{d}t}I(t,\varphi(t,x)) = \partial_t I(t,\varphi(t,x)) + \nabla I(t,\varphi(t,x))^{\mathrm{T}}\partial_t\varphi(t,x),$$
(3)

where  $\nabla$  denotes the gradient with respect to the spatial component in  $\mathbb{R}^d$  and <sup>T</sup> is the transposition of a matrix. By (2), and replacing  $\varphi(t, x) \to x$  for every  $t \in [0, T]$ , the image sequence fulfills the partial differential equation

$$\partial_t I(t,x) + \nabla I(t,x)^{\mathrm{T}} v(t,x) = 0, \qquad (t,x) \in [0,T] \times \Omega,$$

$$I(0,x) = I_0(x), \qquad x \in \Omega,$$
(4)

where  $I_0$  is the first image frame. Note that besides the optical flow, there exist other methods to recover  $\varphi$  related to the general image registration problem (1) capable of larger motion, see [25, 26]. Because the displacement is sufficiently small in our application, it is reasonable to work with the optical flow equation (4), which can be interpreted as a linearization of the registration problem, cf. [13, 45].

For the time-harmonic optical flow elastography [17], the object undergoes a periodic, time-harmonic displacement with frequency  $\omega \in \mathbb{R}$ , which is known from the experimental setup. This implies that the displacement  $u: [0, T] \times \Omega \to \mathbb{R}^d$  in

$$\varphi(t,x) = x + u(t,x) \tag{5}$$

is time-harmonic, i.e.,

$$u(t,x) = \operatorname{Re}(\tilde{a}(x) \operatorname{e}^{\operatorname{i}t\omega}) - \operatorname{Re}(\tilde{a}(x)), \tag{6}$$

with a complex amplitude  $\tilde{a} \in \mathbb{C}$ , where the term  $\operatorname{Re}(\tilde{a}(x))$  comes from the second line of (2). However, if  $\varphi$  is expressed through (5) and (6) and the resulting expression is substituted into (3), it is not clear how to obtain an equation similar to (4) with a linear dependence on  $\tilde{a}$  instead of v. Therefore, we propose to use instead the "ansatz"

$$v(t,x) = \operatorname{Re}\left(a(x) e^{it\omega}\right)$$
  
=  $a_{\mathrm{R}}(x) \cos(t\omega) - a_{\mathrm{I}}(x) \sin(t\omega), \quad t \in [0,T], \ x \in \Omega,$  (7)

where the amplitude  $a = a_{\rm R} + ia_{\rm I}$  with  $a_{\rm R}, a_{\rm I} \in \mathbb{R}$  is again complex and we always assume that a is  $C^2$ . The advantage of this approach is that the systems (2) and (4) are no longer coupled. We first reconstruct a as a solution of (4), where we substitute v by (7), and subsequently obtain the displacement u by solving (2). The relation between both approaches is discussed in the following paragraph.

**Time-harmonic approach with** v **versus** u. Let us consider the relation in the onedimensional case d = 1. In particular, we are interested in the question if the specific time-harmonic structure (7) of the velocity v implies that the deformation  $\varphi$  is also periodic or even that u is time-harmonic as in (6). The following result shows that the first property is fulfilled at least for some choices of the amplitude a.

**Proposition 1 (Time-harmonic amplitude).** Consider for d = 1 the amplitude function

$$a(x) = \alpha(x) e^{i\phi_0} \tag{8}$$

with some locally Lipschitz continuous function  $\alpha \colon \mathbb{R} \to \mathbb{R}$  and some  $\phi_0 \in \mathbb{R}$ . Assume further that  $1/\alpha$  has a bijective antiderivative  $A \colon \mathbb{R} \to \mathbb{R}$ , which is e.g. the case if  $\alpha$ is bounded and bounded away from zero. Then, for every  $x \in \mathbb{R}$ , the displacement is periodic in t and can be expressed as

$$\varphi(t,x) = A^{-1} \left( A(x) + \frac{\sin(t\omega + \phi_0) - \sin(\phi_0)}{\omega} \right).$$
(9)

*Proof:* The corresponding velocity (7) reads as  $v(t, x) = \alpha(x) \cos(t\omega + \phi_0)$ . By (2),  $\varphi$  has to fulfill

$$\frac{\mathrm{d}}{\mathrm{d}t}\varphi(t,x) = \alpha\left(\varphi(t,x)\right)\cos(t\omega + \phi_0), \quad \varphi(0,x) = x.$$

By the Picard–Lindelöf theorem, this initial value problem has a unique solution. Using the separation of variables straightforwardly yields (9).

In the last proposition, a first order Taylor approximation of  $A^{-1}$  around A(x) in (9) yields the approximate displacement

$$u(t,x) = \varphi(t,x) - x \approx \alpha(x) \frac{\sin(t\omega + \phi_0) - \sin(\phi_0)}{\omega},$$

which is a harmonic oscillation of the form (6), so the time-harmonicity is fulfilled at least approximately in this case. If a(x) is constant in the spatial variable x, then  $\varphi(t, x) = x + \text{Im}(ae^{it\omega} - a)/\omega$  is time-harmonic by (9). The following examples show that the situation differs depending on the specific amplitude a.

**Example 2 (Time-harmonic amplitude and periodic deformation).** Let  $a(x) = cx, x \in \mathbb{R}$ , for some  $c \in \mathbb{R}$ . Then the solution of (2) becomes

$$\varphi(t, x) = x e^{-\frac{c}{\omega}\sin(t\omega)},$$



Figure 1: Trajectories  $\varphi(t, x)$  corresponding to the velocity amplitude a(x) = 0.2 x from Example 2 with different starting values x for  $\omega = 1$ .

which is illustrated in Figure 1. In particular, the deformation  $\varphi$  is again  $\frac{2\pi}{\omega}$  periodic in t. An illustration of a two-dimensional example, where the resulting displacement u is periodic, is given in Figure 2.

**Example 3 (Time-harmonic amplitude and non-periodic deformation).** If the amplitude *a* does not have the form (8), the displacement *u* of the motion might be non-periodic. Consider the complex amplitude  $a(x) = e^{-ix}$ ,  $x \in \mathbb{R}$ , and frequency  $\omega = 1$ . Then the velocity is

$$v(t, x) = \operatorname{Re}(e^{i(t-x)}) = \cos(t-x).$$



Figure 2: Two-dimensional images  $I(t, \cdot)$  corresponding to a harmonic velocity (7) with a real-valued amplitude function a and period T = 2000. The displacement uis periodic. The second row is the zoom-in of the first row to the red rectangle. The red • depicts the position  $\varphi(t, x)$  of a single point x at time t and the red curve is its trajectory.



Figure 3: Trajectories  $\varphi(t, x)$  of Example 3 for different starting values x with  $\omega = 1$ .

A straightforward computation using trigonometric identities verifies that

$$\varphi(t,x) = t + 2 \operatorname{arccot}\left(t + \cot\frac{x}{2}\right)$$

for  $x \in (0, \pi)$  is a solution of (2) in this case, in particular we have

$$\frac{\mathrm{d}}{\mathrm{d}t}\varphi(t,x) = 1 - \frac{2}{1 + (t + \cot\frac{x}{2})^2} = \cos(t - \varphi(t,x)).$$

Due to the asymptotics of the inverse cotangent, we have  $\varphi(t, x) \to \infty$  for  $t \to \infty$  and fixed x, cf. Figure 3. Hence, the same holds also for the displacement u(t, x).

An illustration of a two-dimensional example, where the resulting displacement u is non-periodic, is given in Figure 4.



Figure 4: Two-dimensional images  $I(t, \cdot)$  corresponding to a harmonic velocity (7) with an amplitude function of the form  $a(x) \in \mathbb{R} \times \mathbb{R}$  and period T = 2000. The resulting displacement u is not periodic. The second row is the zoom-in of the first row to the red rectangle. The red • depicts the position  $\varphi(t, x)$  of a single point x at time t and the red curve is its trajectory.

An "opposite" example showing a time-harmonic displacement u that results in a periodic velocity v, which is however not time-harmonic, is given in Appendix A.

### 3. Variational models for time-harmonic optical flow

We want to approximate the solution of the flow equation (4) with the time-harmonic velocity field (7) from given measurements I(t, x),  $t \in [0, T]$ ,  $x \in \Omega$ , where we assume that  $\omega > 0$  is known and a full period of the oscillation is observed, i.e.,  $T := 2\pi/\omega$ . More precisely, we aim to recover the amplitude a of the velocity field v. Since the optical flow equation is ill-posed, this is in general tackled by solving a variational problem of the form

$$E(v) \coloneqq \int_{\Omega} \int_{0}^{T} \left( \mathcal{D}\left( \underbrace{\nabla I(t,x)^{\mathrm{T}} v(t,x) + \partial_{t} I(t,x)}_{=:G_{v}(t,x)} \right) + \lambda \mathcal{R}(\nabla v(t,x)) \right) \mathrm{d}t \,\mathrm{d}x, \qquad (10)$$

with a data fidelity term  $\mathcal{D}: \mathbb{R} \to \mathbb{R}_{\geq 0}$  enforcing the physics-based relation (4) and a regularizer  $\mathcal{R}: \mathbb{R}^{d \times d} \to \mathbb{R}_{\geq 0}$ , which aims to make the problem well-posed and contains, from a Bayesian point of view, prior knowledge on the velocity field. Both terms are coupled by a regularization parameter  $\lambda > 0$ . For an overview of data fidelity and regularization terms used in optical flow between two image frames, see e.g. [11]. In this section, we will discuss the following choices:

- I)  $\mathcal{D}(G_v) := |G_v|^2$  and  $\mathcal{R} := \|\nabla v\|^2 = \sum_{j,k=1}^d \left|\partial_{x_j} v_k\right|^2$ ,
- II)  $\mathcal{D}(G_v) \coloneqq |G_v|$  and  $\mathcal{R} \coloneqq \|\nabla v\|$ ,
- III)  $\mathcal{D}(G_v) := |G_v|$  and  $\mathcal{R} := \|\nabla v\|^2$ ,

where  $\|\cdot\|$  denotes the Euclidean norm in  $\mathbb{R}^{d \times d}$ , also known as Frobenius norm. Model I resembles the Horn–Schunck model in image processing [15] and is appropriate for image data corrupted by Gaussian noise and a sufficiently smooth velocity field. Model II is more robust against noise in the image frames, especially heavy-tailed noise stemming, e.g., from the Laplace distribution and also avoids penalizing jumps in the derivative of the velocity field too much, see the total variation model in image denoising [30] and for its counterpart in optical flow, e.g. [1, 14]. Such models appeared to be beneficial for early crack detection in materials in tensile tests [2]. Note that often the above model was only considered for two consecutive image frames and not over the whole sequence of images. Finally, Model III combines the robustness to noise from Model II with the regularization term of Model I and aims for a smoother reconstruction.

In the following, we will show how the Models I – III can be refined using the special timeharmonic structure of the velocity field in (7). In particular, the incorporation of the whole time interval, i.e. of all image frames at the same time, becomes straightforward. To this end, we need the Fourier transform of functions  $f \in L_1(\mathbb{R})$  defined by

$$\mathcal{F}[f](\nu) \coloneqq \int_{\mathbb{R}} f(t) e^{-it\nu} dt, \qquad \nu \in \mathbb{R}.$$
 (11)

If f is supported on [0, T] as it will be the case in our applications, the integral can be just taken over [0, T]. For a vector-valued function f, the Fourier transform is defined componentwise. In what follows, we always apply the Fourier transform in the time variable t and leave the spatial variables fixed.

#### 3.1. Model I

We start by minimizing the functional

$$E(v) \coloneqq \int_{\Omega} \int_0^T \left( |G_v(t,x)|^2 + \lambda \left\| \nabla v(t,x) \right\|^2 \right) \, \mathrm{d}t \, \mathrm{d}x, \tag{12}$$

where we are only interested in the special velocity fields v in (7). Then the minimizer of E(v) is described by the following theorem.

**Theorem 4.** For a given frequency  $\omega \in \mathbb{R}$ , set  $T := 2\pi/\omega$ . Let  $I : [0,T] \times \Omega \to \mathbb{R}$  be an image sequence in  $C^1$  and  $v : [0,T] \times \Omega \to \mathbb{R}^d$  a time-harmonic velocity in  $C^2$  of the form (7). Then, the minimizing amplitude a corresponding to the velocity v in (12) satisfies, for all  $x \in \Omega$ , the equation

$$\lambda T \Delta a(x) = \mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](2\omega, x)\overline{a(x)} + \mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](0, x)a(x) + 2\mathcal{F}[\partial_t I \nabla I](\omega, x), \quad (13)$$

where  $\overline{a}$  denotes the complex conjugate of a and  $\Delta$  is the Laplace operator.

*Proof:* Inserting (7) into E and splitting the amplitude  $a = a_{\rm R} + a_{\rm I}$  as in (7), we obtain

$$E(v) = \int_{\Omega} \int_{0}^{T} \left( \left( \nabla I(t, x)^{\mathrm{T}} a_{\mathrm{R}}(x) \cos(t\omega) - \nabla I(t, x)^{\mathrm{T}} a_{\mathrm{I}}(x) \sin(t\omega) + \partial_{t} I(t, x) \right)^{2} + \lambda \| \nabla a_{\mathrm{R}}(x) \cos(t\omega) - \nabla a_{\mathrm{I}}(x) \sin(t\omega) \|^{2} \right) \, \mathrm{d}t \, \mathrm{d}x.$$

Since we integrate over a full period, this becomes

$$E(v) = \int_{\Omega} \left( \int_{0}^{T} \left( \nabla I(t, x)^{\mathrm{T}} a_{\mathrm{R}}(x) \cos(t\omega) - \nabla I(t, x)^{\mathrm{T}} a_{\mathrm{I}}(x) \sin(t\omega) + \partial_{t} I(t, x) \right)^{2} \mathrm{d}t + \frac{\lambda T}{2} \left( \| \nabla a_{\mathrm{R}}(x) \|^{2} + \| \nabla a_{\mathrm{I}}(x) \|^{2} \right) \right) \mathrm{d}x.$$

$$(14)$$

The Euler-Lagrange equations yield that the minimizer a has to satisfy for all i = 1, ..., d the equations

$$\begin{split} \lambda T \sum_{j=1}^{d} \partial_{x_j}^2(a_{\mathrm{R}})_i(x) &= \int_0^T 2 \Big( \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{R}}(x) \cos(t\omega) - \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{I}}(x) \sin(t\omega) \\ &+ \partial_t I(t,x) \Big) \, \partial_{x_i} I(t,x) \cos(t\omega) \, \mathrm{d}t, \\ \lambda T \sum_{j=1}^{d} \partial_{x_j}^2(a_{\mathrm{I}})_i(x) &= \int_0^T 2 \Big( \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{R}}(x) \cos(t\omega) - \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{I}}(x) \sin(t\omega) \\ &+ \partial_t I(t,x) \Big) \, \Big( - \partial_{x_i} I(t,x) \sin(t\omega) \Big) \, \mathrm{d}t. \end{split}$$

Using trigonometric identities  $2\cos^2(y) = 1 + \cos(2y)$  and  $2\sin^2(y) = 1 - \cos(2y)$ , we can equivalently state the last equations in vector form as

$$\begin{split} \lambda T \Delta a_{\mathrm{R}}(x) &= \int_{0}^{T} \nabla I(t,x) \left( \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{R}}(x) (1 + \cos(2t\omega)) \right. \\ &\quad - \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{I}}(x) \sin(2t\omega) + \partial_{t} I(t,x) 2 \cos(t\omega) \right) \mathrm{d}t \\ \lambda T \Delta a_{\mathrm{I}}(x) &= \int_{0}^{T} \nabla I(t,x) \left( - \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{R}}(x) \sin(2t\omega) \right. \\ &\quad + \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{I}}(x) (1 - \cos(2t\omega)) - \partial_{t} I(t,x) 2 \sin(t\omega) \right) \mathrm{d}t. \end{split}$$

Then, the temporal Fourier transform (11) yields

$$\lambda T \Delta a_{\mathrm{R}}(x) = \left( \mathrm{Re}\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](0, x) + \mathrm{Re}\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](2\omega, x) \right) a_{\mathrm{R}}(x) + \mathrm{Im}\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](2\omega, x) a_{\mathrm{I}}(x) + 2\mathrm{Re}\mathcal{F}[\partial_{t}I \nabla I](\omega, x), \lambda T \Delta a_{\mathrm{I}}(x) = \left( \mathrm{Re}\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](0, x) - \mathrm{Re}\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](2\omega, x) \right) a_{\mathrm{I}}(x) + \mathrm{Im}\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](2\omega, x) a_{\mathrm{R}}(x) + 2\mathrm{Im}\mathcal{F}[\partial_{t}I \nabla I](\omega, x).$$

Since  $I(t, x) \in \mathbb{R}$ , we get  $\mathcal{F}[\nabla I \nabla I^{\mathrm{T}}](0, x) \in \mathbb{R}^{d \times d}$ . By returning to the complex-valued function a, we get the assertion.

As the unknown a depends only on the spatial variable x and the Fourier coefficients of the derivatives of I can be precomputed, the size of the linear system (13) is independent of the time period T. This causes a significant runtime improvement compared to the estimation of the optical flow velocity between all consecutive pairs of images.

**Remark 5 (Wirtinger derivatives).** The derivation of (13) could be slightly shortened by using the chain rule and Euler–Lagrange equations for complex Wirtinger derivatives [47]. Calculating (13) in terms of real and imaginary parts of a was also done for implementation purposes.

#### 3.2. Model II

For Model II, the functional (10) becomes

$$E(v) \coloneqq \int_{\Omega} \int_0^T \left( |G_v(t, x)| + \lambda \|\nabla v(t, x)\| \right) \, \mathrm{d}t \, \mathrm{d}x.$$
(15)

The data fidelity term resembles the  $L_1$  norm on  $[0, T] \times \Omega$  and is also known as *least* absolute deviations [8]. A modified  $L_1$  term has been applied in optical flow estimation between two images [9]. In particular, they used the Charbonnier penalty  $\mathcal{D}(G_v) = \sqrt{|G_v|^2 + \varepsilon^2}$  for some  $\varepsilon > 0$  as a part of their data fidelity term. The regularizer can be seen as the vectorial total variation (TV) norm of v, see [12, eq. (9)].

As (15) is no longer differentiable, finding its minimizer via Euler-Lagrange equations is not possible. While a variety of optimization techniques for (15) exist, we adopt to our setting a majorize-minimize technique known as the *iteratively reweighted least squares* (IRLS) [19, 23] or half-quadratic minimization [7]. For each iteration of the algorithm, a global quadratic majorant of (15) depending on the current iterate is constructed. Then it is minimized and its optimizer is set to be the next iterate. For each iteration, we are required to precompute the quadratic majorant only once and then minimize it efficiently akin to Model I. As a result, we only need a few costly precomputations unlike other optimization methods requiring frequent evaluations of the complete (time-dependent) velocity v.

To construct a majorant of (15), we consider the Huber function

$$h_{\varepsilon} \colon \mathbb{R} \to \left[\frac{\varepsilon}{2}, \infty\right), \quad x \mapsto \begin{cases} |x|, & |x| \ge \varepsilon, \\ \frac{|x|^2}{2\varepsilon} + \frac{\varepsilon}{2}, & |x| < \varepsilon, \end{cases}$$

with smoothing parameter  $\varepsilon > 0$ . It is a smoothed version of |x| linked to its Moreau envelope [5, Examples 6.54 and 6.62] and satisfies the following properties.

**Lemma 6.** Let  $x, z \in \mathbb{R}$ . For all  $0 < \varepsilon_1 \leq \varepsilon_2$ , we have

$$h_{\varepsilon_1}(x) \leq h_{\varepsilon_2}(x)$$
 and  $\lim_{\varepsilon \downarrow 0} h_{\varepsilon}(x) = |x|.$ 

Next, we replace  $|\cdot|$  by  $h_{\varepsilon}$  in the energy functional (15). We consider the smoothed energy functional

$$E_{\varepsilon,\delta}(v) \coloneqq \int_{\Omega} \int_{0}^{T} \left( h_{\varepsilon} \left( G_{v}(t,x) \right) \right) + \lambda h_{\delta} \left( \left\| \nabla v(t,x) \right\| \right) \right) \, \mathrm{d}t \, \mathrm{d}x \ge E(v),$$

with data fidelity and regularization smoothing parameters  $\varepsilon, \delta > 0$ . It is a majorant of E(v), however, it is not a quadratic functional. Thus, we proceed further by utilizing the following lemma.

**Lemma 7** ([19, Lem. 2.1]). Let  $x, z \in \mathbb{R}$  and  $\varepsilon > 0$ . Define

$$q_{\varepsilon}(x,z) \coloneqq \frac{|x|^2}{2\max\{\varepsilon, |z|\}} + \frac{1}{2}\max\{\varepsilon, |z|\}.$$
(16)

Then,  $q_{\varepsilon}$  is a quadratic majorant of  $h_{\varepsilon}$  satisfying

$$h_{\varepsilon}(x) \leq q_{\varepsilon}(x,z)$$
 and  $h_{\varepsilon}(x) = q_{\varepsilon}(x,x).$ 

For  $u: [0,T] \times \Omega \to \mathbb{R}^d$ , we set

$$E_{u,\varepsilon,\delta}(v) \coloneqq \int_{\Omega} \int_{0}^{T} \left( q_{\varepsilon} \left( G_{v}(t,x), G_{u}(t,x) \right) + \lambda q_{\delta} \left( \left\| \nabla v(t,x) \right\|, \left\| \nabla u(t,x) \right\| \right) \right) \, \mathrm{d}t \, \mathrm{d}x.$$
(17)

Then we have

$$E(v) \leq E_{\varepsilon,\delta}(v) \leq E_{u,\varepsilon,\delta}(v).$$

The iteration

$$v^{k+1} = \operatorname*{arg\,min}_{v^{k},\varepsilon,\delta}(v), \qquad k \in \mathbb{N}_{0},$$

leads to

$$E_{\varepsilon,\delta}(v^{k+1}) \leqslant E_{v^k,\varepsilon,\delta}(v^{k+1}) \leqslant E_{v^k,\varepsilon,\delta}(v^k) = E_{\varepsilon,\delta}(v^k)$$
(18)

and the values  $E_{\varepsilon,\delta}(v^k)$  form a nonincreasing convergent sequence for  $k \to \infty$ . For fixed parameters  $\varepsilon$  and  $\delta$ , this procedure only minimizes  $E_{\varepsilon,\delta}$  instead of (15). Since  $E_{\varepsilon,\delta}$  goes to E as the smoothing parameters vanish, a common strategy is to take sequences  $\varepsilon_k, \delta_k \downarrow 0$ and construct the iterates

$$v^{k+1} \coloneqq \operatorname*{arg\,min}_{v} E_{v^k,\varepsilon^k,\delta^k}(v)$$

This step does not affect the convergence argument in (18) as

$$E_{\varepsilon^{k+1},\delta^{k+1}}(v^{k+1}) \leqslant E_{\varepsilon^k,\delta^k}(v^{k+1}) \leqslant E_{\varepsilon^k,\delta^k}(v^k).$$

A more advanced derivation [23, Thm. 6] shows that (in a slightly different setting) with a proper decay strategy of  $\varepsilon^{k+1}$ ,  $\delta^{k+1}$ , the iterates  $v^k$  are guaranteed to converge to a global minimum of E(v) at a sublinear rate  $\mathcal{O}(k^{-\frac{1}{3}})$ . Furthermore, with an additional assumption, a linear convergence is achievable [23, Thm. 9].

Now we focus on the minimization of  $E_{v^k,\varepsilon^k,\delta^k}$ . In fact, it can be seen as a weighted version of (13).

**Theorem 8.** Let  $\varepsilon, \delta > 0$  and  $u: [0,T] \times \Omega \to \mathbb{R}^d$  in  $C^1$  be fixed. Consider the flow velocity  $v(t,x) = \operatorname{Re}(a(x)e^{i\omega t})$  in  $C^2$ . Then the amplitude  $a: \Omega \to \mathbb{C}^d$  of the minimizer v of  $E_{u,\varepsilon,\delta}(v)$ , see (17), satisfies

$$\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](0,x)a(x) + \mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](2\omega,x)\overline{a(x)} + 2\mathcal{F}[w_{\mathcal{D}}\partial_{t}I\nabla I](\omega,x)$$
$$= \lambda \sum_{j=1}^{d} \partial_{x_{j}} \left(\mathcal{F}[w_{\mathcal{R}}](0,x)\partial_{x_{j}}a(x) + \mathcal{F}[w_{\mathcal{R}}](2\omega,x)\overline{\partial_{x_{j}}a(x)}\right)$$
(19)

for all  $x \in \Omega$ , where  $w_{\mathcal{D}}, w_{\mathcal{R}} \colon [0, T] \times \Omega \to \mathbb{R}$  are defined by

$$w_{\mathcal{D}}(t,x) \coloneqq \frac{1}{\max\{\varepsilon, |G_u(t,x)|\}} \quad and \quad w_{\mathcal{R}}(t,x) \coloneqq \frac{1}{\max\{\delta, \|\nabla u(t,x)\|\}}.$$
 (20)

*Proof:* As the second term in the definition (16) of  $q_{\varepsilon}(x, z)$  does not depend on x, we can write  $E_{u,\varepsilon,\delta}(v)$  as

$$E_{u,\varepsilon,\delta}(v) = \frac{1}{2} \int_{\Omega} \int_{0}^{T} \left( \frac{|G_v(t,x)|^2}{\max\{\varepsilon, |G_u(t,x)|\}} + \lambda \frac{\|\nabla v(t,x)\|^2}{\max\{\delta, \|\nabla u(t,x)\|\}} \right) dt dx + \text{const}$$
$$= \frac{1}{2} \int_{\Omega} \int_{0}^{T} w_{\mathcal{D}}(t,x) |G_v(t,x)|^2 + \lambda w_{\mathcal{R}}(t,x) \|\nabla v(t,x)\|^2 dt dx + \text{const.}$$

We first want to compute the regularization term

$$R(a(x)) := \int_0^T w_{\mathcal{R}}(t,x) \|\nabla v(t,x)\|^2 \, \mathrm{d}t.$$

Substituting  $v(t, x) = \operatorname{Re}(a(x)e^{i\omega t})$  gives

$$\begin{aligned} \left\|\nabla v(t,x)\right\|^{2} &= \left\|\operatorname{Re}(\nabla a(x)\mathrm{e}^{\mathrm{i}\omega t})\right\|^{2} \\ &= \frac{1}{4} \left\|\nabla a(x)\mathrm{e}^{\mathrm{i}\omega t} + \overline{\nabla a}(x)\mathrm{e}^{-\mathrm{i}\omega t}\right\|^{2} \\ &= \frac{1}{2} \left\|\nabla a(x)\right\|^{2} + \frac{1}{2}\operatorname{Re}\left(\left\langle\nabla a(x)\mathrm{e}^{\mathrm{i}\omega t}, \overline{\nabla a}(x)\mathrm{e}^{-\mathrm{i}\omega t}\right\rangle_{\mathrm{Fro}}\right) \\ &= \frac{1}{2} \left\|\nabla a(x)\right\|^{2} + \frac{1}{2}\operatorname{Re}\left(\sum_{k,j=1}^{d} (\partial_{x_{j}}a_{k}(x))^{2}\mathrm{e}^{2\mathrm{i}\omega t}\right). \end{aligned}$$

Integrating over t yields

$$R(a(x)) = \frac{1}{2} \int_0^T w_{\mathcal{R}}(t,x) \left[ \|\nabla a(x)\|^2 + \operatorname{Re}\left(\sum_{k,j=1}^d (\partial_{x_j} a_k(x))^2 \mathrm{e}^{2\mathrm{i}\omega t}\right) \right]$$
$$= \frac{1}{2} \mathcal{F}[w_{\mathcal{R}}](0,x) \|\nabla a(x)\|^2 + \frac{1}{2} \operatorname{Re}\left(\sum_{k,j=1}^d (\partial_{x_j} a_k(x))^2 \mathcal{F}[w_{\mathcal{R}}](-2\omega,x)\right)$$
$$= \frac{1}{2} \mathcal{F}[w_{\mathcal{R}}](0,x) \|\nabla a(x)\|^2 + \frac{1}{2} \operatorname{Re}\left(\sum_{k,j=1}^d (\partial_{x_j} a_k(x))^2 \overline{\mathcal{F}[w_{\mathcal{R}}]}(2\omega,x)\right),$$

where in the last line we used that the temporal Fourier transform of the real-valued  $w_{\mathcal{R}}$  is conjugate symmetric. Splitting  $a = a_{\mathrm{R}} + \mathrm{i}a_{\mathrm{I}}$  into its real and imaginary parts, we obtain

$$\|\nabla a(x)\|^2 = \sum_{k,j=1}^d (\partial_{x_j}(a_{\mathbf{R}})_k(x))^2 + (\partial_{x_j}(a_{\mathbf{I}}(x))_k)^2$$

and

$$\operatorname{Re}\left(\sum_{k,j=1}^{d} (\partial_{x_{j}}a_{k}(x))^{2}\overline{\mathcal{F}[w_{\mathcal{R}}]}(2\omega, x)\right)$$
$$=\sum_{k,j=1}^{d} \operatorname{Re}\left((\partial_{x_{j}}a_{k}(x))^{2}\right) \operatorname{Re}\mathcal{F}[w_{\mathcal{R}}](2\omega, x) + \operatorname{Im}\left((\partial_{x_{j}}a_{k}(x))^{2}\right) \operatorname{Im}\mathcal{F}[w_{\mathcal{R}}](2\omega, x)$$
$$=\sum_{k,j=1}^{d} \left((\partial_{x_{j}}(a_{\mathrm{R}})_{k}(x))^{2} - (\partial_{x_{j}}(a_{\mathrm{I}})_{k}(x))^{2}\right) \operatorname{Re}\mathcal{F}[w_{\mathcal{R}}](2\omega, x)$$
$$+ 2\partial_{x_{j}}(a_{\mathrm{R}})_{k}(x)\partial_{x_{j}}(a_{\mathrm{I}})_{k}(x) \operatorname{Im}\mathcal{F}[w_{\mathcal{R}}](2\omega, x).$$

Combining all the terms and rearranging the summands ultimately gives the regularizer

$$R(\nabla a(x)) = \sum_{k,j=1}^{d} \frac{1}{2} \left( \mathcal{F}[w_{\mathcal{R}}](0,x) + \operatorname{Re}\mathcal{F}[w_{\mathcal{R}}](2\omega,x) \right) \left( \partial_{x_{j}}(a_{\mathrm{R}})_{k}(x) \right)^{2}$$
$$+ \sum_{k,j=1}^{d} \frac{1}{2} \left( \mathcal{F}[w_{\mathcal{R}}](0,x) - \operatorname{Re}\mathcal{F}[w_{\mathcal{R}}](2\omega,x) \right) \left( \partial_{x_{j}}(a_{\mathrm{I}})_{k}(x) \right)^{2}$$
$$+ \sum_{k,j=1}^{d} \operatorname{Im}\mathcal{F}[w_{\mathcal{R}}](2\omega,x) \partial_{x_{j}}(a_{\mathrm{R}})_{k}(x) \partial_{x_{j}}(a_{\mathrm{I}})_{k}(x).$$

The data fidelity term is transformed analogously to Theorem 4 resulting in

$$D(a(x)) \coloneqq \int_0^T w_{\mathcal{D}}(t,x) |G_v(t,x)|^2$$
  
= 
$$\int_0^T w_{\mathcal{D}}(t,x) \left(\nabla I(t,x)^{\mathrm{T}} a_{\mathrm{R}}(x) \cos(t\omega) + \nabla I(t,x)^{\mathrm{T}} a_{\mathrm{I}}(x) \sin(-t\omega) + \partial_t I(t,x)\right)^2 \mathrm{d}t.$$

In summary, the functional  $E_{u,\varepsilon,\delta}(v)$  becomes

$$E_{u,\varepsilon,\delta}(v) = \frac{1}{2} \int_{\Omega} D(a(x)) + \lambda R(\nabla a(x)) \, \mathrm{d}x + \text{const.}$$

The Euler-Lagrange equations are then given by

$$\frac{\partial D(a(x))}{\partial (a_{\mathrm{R}})_{k}} = \lambda \sum_{j=1}^{d} \partial_{x_{j}} \frac{\partial R(\nabla a(x))}{\partial (\partial_{x_{j}}(a_{\mathrm{R}})_{k}(x))},$$
$$\frac{\partial D(a(x))}{\partial (a_{\mathrm{I}})_{k}} = \lambda \sum_{j=1}^{d} \partial_{x_{j}} \frac{\partial R(\nabla a(x))}{\partial (\partial_{x_{j}}(a_{\mathrm{I}})_{k}(x))},$$

for all  $k \in [d]$ . The left-hand side can be transformed similarly to the proof of Theorem 4 with  $w_{\mathcal{D}}(t, x)$  entering the Fourier coefficients,

$$\frac{\partial D(a(x))}{\partial a_{\mathrm{R}}} = \left( \mathrm{Re}\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](0,x) + \mathrm{Re}\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](2\omega,x) \right) a_{\mathrm{R}}(x) \\
+ \mathrm{Im}\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](2\omega,x)a_{\mathrm{I}}(x) + 2\mathrm{Re}\mathcal{F}[w_{\mathcal{D}}\partial_{t}I\nabla I](\omega,x), \\
\frac{\partial D(a(x))}{\partial a_{\mathrm{I}}} = \left( \mathrm{Re}\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](0,x) - \mathrm{Re}\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](2\omega,x) \right) a_{\mathrm{I}}(x) \\
+ \mathrm{Im}\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](2\omega,x)a_{\mathrm{R}}(x) + 2\mathrm{Im}\mathcal{F}[w_{\mathcal{D}}\partial_{t}I\nabla I](\omega,x).$$

The right-hand side reads as

$$\begin{split} \sum_{j=1}^{d} \partial_{x_j} \frac{\partial R(\nabla a(x))}{\partial (\partial_{x_j}(a_{\mathrm{R}})_k(x))} &= \sum_{j=1}^{d} \partial_{x_j} \left( (\mathcal{F}[w_{\mathcal{R}}](0,x) + \mathrm{Re}\mathcal{F}[w_{\mathcal{R}}](2\omega,x)) \,\partial_{x_j}(a_{\mathrm{R}})_k(x) \right) \\ &+ \sum_{j=1}^{d} \partial_{x_j} \left( \mathrm{Im}\mathcal{F}[w_{\mathcal{R}}](2\omega,x) \partial_{x_j}(a_{\mathrm{I}})_k(x) \right) , \\ \sum_{j=1}^{d} \partial_{x_j} \frac{\partial R(\nabla a_{\mathrm{R}}(x), \nabla a_{\mathrm{I}}(x))}{\partial (\partial_{x_j}(a_{\mathrm{I}})_k(x))} &= \sum_{j=1}^{d} \partial_{x_j} \left( (\mathcal{F}[w_{\mathcal{R}}](0,x) - \mathrm{Re}\mathcal{F}[w_{\mathcal{R}}](2\omega,x)) \,\partial_{x_j}(a_{\mathrm{I}})_k(x) \right) \\ &+ \sum_{j=1}^{d} \partial_{x_j} \left( \mathrm{Im}\mathcal{F}[w_{\mathcal{R}}](2\omega,x) \partial_{x_j}(a_{\mathrm{R}})_k(x) \right) . \end{split}$$

Combining  $a_{\mathrm{R}}$  and  $a_{\mathrm{I}}$  into a and noticing that  $\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](0,x) \in \mathbb{R}^{d \times d}$  yields the desired system.

The reconstruction process is summarized in Algorithm 1. Similarly to Model I, the size of the linear system (19) is independent of the time period T. However, in this case, the weights  $w_{\mathcal{D}}$  and  $w_{\mathcal{R}}$  are time-dependent and, thus, finding a solution to Model II with Algorithm 1 is expected to be slower than to Model I. However, if the number of IRLS iterations K is small, this difference is less pronounced.

#### Algorithm 1: IRLS for Model II

**Data:** Images I, initial guess  $a^0$ , starting smoothing parameters  $\varepsilon^0, \delta^0 > 0$ , number of iterations  $K \in \mathbb{N}$ . **Result:** Reconstructed density a. **for**  $k = 0, \dots, K - 1$  **do** Compute the velocity  $v^k(t, x) = \operatorname{Re}(a^k(x)e^{it\omega})$ . Compute the weights  $w_{\mathcal{D}}$  and  $w_{\mathcal{R}}$  from (20) with  $v^k$ ,  $\varepsilon^k$  and  $\delta^k$ . Compute  $a^{k+1}$ , which is the minimizer of  $E_{v^k,\varepsilon^k,\delta^k}$ , by solving (19). Update  $\varepsilon^{k+1}, \delta^{k+1}$  such that  $\varepsilon^{k+1} \leq \varepsilon^k, \delta^{k+1} \leq \delta^k$ . Set  $a = a^K$ . We briefly discuss our update rule for the smoothing parameters  $\varepsilon^k$ ,  $\delta^k$  assuming that  $\Omega$  has finite volume  $|\Omega|$ . They are chosen as the minimum between the previous values and the scaled average of the current residual, i.e.,

$$\varepsilon^{k+1} = \max\left\{\min\left\{\varepsilon^{k}, \frac{0.1}{T|\Omega|\sqrt{k+1}}\int_{\Omega}\int_{0}^{T}|G_{v}(t,x)|\,\mathrm{d}t\,\mathrm{d}x\right\}, \frac{c}{\sqrt{k+1}}\right\},\\\delta^{k+1} = \max\left\{\min\left\{\delta^{k}, \frac{0.1}{T|\Omega|\sqrt{k+1}}\int_{\Omega}\int_{0}^{T}\|\nabla v(t,x)\|\,\mathrm{d}t\,\mathrm{d}x\right\}, \frac{c}{\sqrt{k+1}}\right\},$$

where  $c = 10^{-8}$  is a small constant. The role of the maximum is to prevent the smoothing parameters from becoming zero. This choice does not come with theoretical convergence guarantees, but it resembles the choices in [23, Thm. 6 and 9]. For a more comprehensive overview of possible strategies, we refer to [23, § 7.1]. Other than the decay strategy of the smoothing parameters, IRLS has no hyperparameters to tune, which makes its implementation and use straightforward compared to ADMM-based or primal-dual methods.

#### 3.3. Model III

Model III combines the approaches of the two previous sections by taking the  $L_1$  data fidelity term (least absolute deviations), which is more robust to outliers, and the  $L_2$ regularizer, which promotes the smoothness of the reconstructed a. In particular, we consider the energy functional

$$E(v) \coloneqq \int_{\Omega} \int_{0}^{T} \left( |G_{v}(t,x)| + \lambda \|\nabla v(t,x)\|^{2} \right) dt dx$$
$$= \int_{\Omega} \left( \int_{0}^{T} |G_{v}(t,x)| dt + \frac{\lambda T}{2} \|\nabla a(x)\|^{2} \right) dx.$$

Note that the data fidelity term scales linearly in v, while the regularizer scales quadratically. This leads to a signal- and noise-level dependent choice of the regularization parameter  $\lambda$ , unlike in the previous two scenarios.

The minimization can be performed with the IRLS method similarly to Section 3.2. Analogously to (17), we define for  $\varepsilon > 0$  and  $u, v \colon [0, T] \times \Omega \to \mathbb{R}^d$  a quadratic majorant of E at u by

$$E_{u,\varepsilon}(v) := \int_{\Omega} \int_{0}^{T} \left( q_{\varepsilon} \left( G_{v}(t,x), G_{u}(t,x) \right) + \lambda \left\| \nabla u(t,x) \right\|^{2} \right) \, \mathrm{d}t \, \mathrm{d}x, \tag{21}$$

with  $q_{\varepsilon}$  from (16). Then, the functional (21) is iteratively minimized as in Algorithm 1. The following theorem can be shown along the lines of Theorem 8 with  $w_{\mathcal{R}} \equiv 2$ .

**Theorem 9.** Let  $\varepsilon > 0$  and  $u: [0,T] \times \Omega \to \mathbb{R}^d$  in  $C^1$  be fixed. Consider the flow velocity  $v(t,x) = \operatorname{Re}(a(x)e^{i\omega t})$  in  $C^2$ . Then the amplitude  $a: \Omega \to \mathbb{C}^d$  of the minimizer v of (21) satisfies

$$\mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](0,x)a(x) + \mathcal{F}[w_{\mathcal{D}}\nabla I\nabla I^{\mathrm{T}}](2\omega,x)\overline{a(x)} + 2\mathcal{F}[w_{\mathcal{D}}\partial_{t}I\nabla I](\omega,x)$$
  
=  $2\lambda T\Delta a(x)$  (22)

for all  $x \in \Omega$ , where  $\mathcal{F}$  is the temporal Fourier transform (11) and

$$w_{\mathcal{D}}(t,x) = \frac{1}{\max\{\varepsilon, |G_u(t,x)|\}}.$$

In (21), the quadratic majorant  $q_{\varepsilon}$  includes an additional factor of  $\frac{1}{2}$  while the regularization term does not. It leads to an extra factor 2 in the right-hand side of (22) or, equivalently,  $w_{\mathcal{R}} \equiv 2$ . This is not the case for Model II, where the majorant  $q_{\varepsilon}$  is used for both data fidelity and regularization term. Hence, the factor  $\frac{1}{2}$  has no impact on (13).

The solution to Model III can be found analogously to Algorithm 1, where  $w_{\mathcal{R}} \equiv 2$ , the parameter  $\delta$  does not appear and the linear system (22) is solved instead of (19).

### 4. Numerical Implementation

In this section, we summarize implementation details for the numerical realization of our minimization procedure. Most of these are somehow standard in optical flow computation, but have to be adapted to our setting. We refer to [38] for an extensive numerical comparison of several of these methods.

Discretization. We work in dimension d = 2 with discrete images of size  $n_1 \times n_2$ . The images can be seen as pointwise evaluations of the respective functions on a grid  $\Gamma := [n_1] \times [n_2]$  with notation  $[n] = \{1, \ldots, n\}$ . Consequently, in the implementation, all integrals  $\int_{\Omega} dx$  are replaced by sums over the grid  $\sum_{x \in \Gamma}$ . Similarly, the images do not form a continuum in the time variable, and thus we use  $t \in [T]$  for  $T \in \mathbb{N}$  time steps. Henceforth, we consider a discrete image as a 3D tensor  $\mathbf{I} = [I(t, x)]_{t \in [T], x \in \Gamma} \in \mathbb{R}^{T \times n_1 \times n_2}$ . We discretize the temporal Fourier transform (11) by

$$\boldsymbol{F}[\boldsymbol{I}](\nu, x) = \frac{1}{T} \sum_{t=0}^{T-1} I(t, x) e^{-it\nu}, \qquad (\nu, x) \in [T] \times \Gamma.$$
(23)

Derivatives. For the discrete approximation of the derivatives, we distinguish between  $\nabla a$  and  $\nabla I$ . The partial derivative  $\partial_1 I$  is approximated via an image filtering  $\mathbf{I} \star \mathbf{h}_c$  in

the spatial coordinates as follows. The convolution with the kernel

$$\boldsymbol{h}_{\mathrm{c}} = rac{1}{8} \begin{bmatrix} -1 & -2 & -1 \\ 0 & 0 & 0 \\ 1 & 2 & 1 \end{bmatrix},$$

which is also known as the Sobel filter, is defined by

$$\boldsymbol{D}_{c,1}\boldsymbol{I} \coloneqq \boldsymbol{I} \star \boldsymbol{h}_{c}(t;k,j) \coloneqq \sum_{p,q=-1}^{1} \boldsymbol{I}(t;k+p,j+q) \boldsymbol{h}_{c}(p,q), \qquad (k,j) \in \Gamma, \ t \in [T], \ (24)$$

where  $\boldsymbol{I}$  is padded by zeros. Note that we index the elements of the matrix  $\boldsymbol{h}_{c}$  from -1 to 1 in order to obtain central derivatives. Analogously, we approximate  $\partial_{2}I$  by  $\boldsymbol{I} \star \boldsymbol{h}^{\mathrm{T}}$ . For derivatives of  $\boldsymbol{a}$  and time derivative of  $\boldsymbol{I}$ , we use forward differences associated with the filter kernel  $\boldsymbol{h}_{\mathrm{fwd}} = \begin{bmatrix} 0 & -1 & 1 \end{bmatrix}^{\mathrm{T}}$ , i.e., with the *i*-th component  $\boldsymbol{a}_{i} = [a_{i}(x)]_{x\in\Gamma}$ , i = 1, 2, we approximate  $\partial_{1}a_{i}(k, j)$  by

$$\boldsymbol{D}_{1}\boldsymbol{a}_{i}(k,j) \coloneqq \boldsymbol{a}_{i} \star \boldsymbol{h}_{\text{fwd}}(k,j) = \boldsymbol{a}_{i}(k+1,j) - \boldsymbol{a}_{i}(k,j), \qquad (k,j) \in \Gamma, \qquad (25)$$

if  $k < n_1$ , and we set  $\boldsymbol{D}_1 \boldsymbol{a}_i(n_1, j) \coloneqq 0$ .

In contrast to the forward differences, the usage of central differences for  $\nabla a$  leads to reconstruction artifacts in our simulations. This is likely caused by the fact that our algorithms require the computation of  $\boldsymbol{D}_1^{\mathrm{T}} \boldsymbol{D}_1 \boldsymbol{a}(k,j) = \boldsymbol{a}(k+1,j) + \boldsymbol{a}(k-1,j) - 2\boldsymbol{a}(k,j)$ , which is a good approximation of the second derivative in (13).

Least squares implementation. Unlike in the classical Horn–Schunck method, which is outlined in Appendix B, we solve the linear system (13) directly. That is, with  $\boldsymbol{a} = \boldsymbol{a}_{\mathrm{R}} + \mathrm{i}\boldsymbol{a}_{\mathrm{I}} \in \mathbb{C}^{2 \times n_1 \times n_2}$  and the vectorization operator vec:  $\mathbb{R}^{2 \times n_1 \times n_2} \to \mathbb{R}^{2n_1n_2}$ , the linear system (13) can be discretized in the form

$$\boldsymbol{C}\begin{bmatrix}\operatorname{vec}(\boldsymbol{a}_{\mathrm{R}})\\\operatorname{vec}(\boldsymbol{a}_{\mathrm{I}})\end{bmatrix} = \boldsymbol{b},$$
(26)

where **b** depends only on the data **I** and the matrix **C** depends on the data **I** and the regularization parameter  $\lambda$ . The construction of **C** and **b** for the case d = 1 is outlined in Appendix C, where we see that the square matrix **C** is symmetric positive semidefinite.

As the multiplication with C can be efficiently computed, this allows for the use of standard Matlab solvers such as the conjugate gradient (CG) method pcg, cf. [3]. Similarly, equations (19) and (22) corresponding to Model II and III, respectively, are weighted versions of (13) and can be rewritten analogously in the matrix form (26).

Computational complexity. For Model I, the CG method is applied to find a solution of (26). To this end, we precompute **b** and Fourier coefficients in **C** at the expense of  $\mathcal{O}(Tn_1n_2)$  operations, see Appendix C for details. Note that we do not need to compute

the full fast Fourier transform, which would give all frequencies, since we need only the frequencies 0,  $\omega$  and  $2\omega$ , for which the sum (23) is evaluated directly. The computational complexity of a single CG iteration is proportional to the cost of a matrix-vector product with the sparse matrix C, which has a complexity of  $\mathcal{O}(n_1n_2)$ . Consequently, for Model I performing  $K_{\rm CG}$  iterations of the CG method, the total computational complexity is  $\mathcal{O}((T + K_{\rm CG})n_1n_2)$ .

For Models II and III, Algorithm 1 is implemented. For each IRLS iteration, the computation of the velocity  $v^k$  from given  $a^k$ , the weights  $w_{\mathcal{D}}, w_{\mathcal{R}}$  by (20) and the update of the smoothing parameters  $\varepsilon$ ,  $\delta$  require a total of  $\mathcal{O}(Tn_1n_2)$  operations. Solving the resulting linear system has the same cost as in Model I, i.e.,  $\mathcal{O}((T + K_{\rm CG})n_1n_2)$ . Hence, running Models II and III for  $K_{\rm irls}$  IRLS iterations and  $K_{\rm CG}$  inner CG iterations requires  $\mathcal{O}(K_{\rm IRLS}(T + K_{\rm CG})n_1n_2)$  operations. The constant in big  $\mathcal{O}$  notation is a little smaller for Model III than for Model II because  $w_{\mathcal{R}}$  is constant and a part of the computations is not required.

*Preprocessing.* As a preprocessing step, the images are smoothed with a Gaussian kernel of standard deviation  $\sigma = 0.65$ . This step both filters out noise and smoothens sharp edges in the images, which have a strong impact on the reconstruction quality.

Coarse-to-fine pyramid. We adopt the coarse-to-fine approach discussed in [37, § 4.2], which consists in constructing a pyramid of images  $\mathbf{I}^{\ell}$  as follows. Starting with the top level L as the initial image sequence  $\mathbf{I}^{(L)} = \mathbf{I}$ , the next level  $\mathbf{I}^{(\ell)}$  is obtained by smoothing  $\mathbf{I}^{(\ell+1)}$  with a Gaussian kernel and downsampling it with the factor  $\eta$  such that  $\mathbf{I}^{(L-1)} \in \mathbb{R}^{T \times [\eta n_1] \times [\eta n_2]}$  and so on. The standard deviation of the Gaussian kernel is commonly chosen as  $\sigma = 1/\sqrt{2\eta}$ .

The reconstruction starts with the smallest image  $I^{(1)}$ . In each level  $\ell \in [L]$ , we compute  $v^{(\ell)}$  as solution of the optical flow problem with the image  $I^{(\ell)}$ , where we use as initialization in the  $\ell$ -th level the appropriately rescaled reconstruction  $v^{(\ell-1)}$ . This yields a faster recovery as we need fewer CG iterations in each level due to the initialization.

Median filtering. As a postprocessing step, a  $5 \times 5$  median filter is applied to the reconstructions  $v^{(\ell)}$  obtained at each level of the coarse-to-fine pyramid.

Warping of derivatives. The coarse-to-fine approach provides intermediate solutions  $v^{(\ell)}$  at each level  $\ell \in [L]$ . As these estimated velocities are good approximations of v, they can be used to obtain a better approximation of the derivative  $\nabla I$  in the variational model (10), see [2, § 2.1].

Denote by  $\tilde{v}(t, x)$  the estimated velocity from the previous level. The first-order Taylor approximation of  $\varphi$  yields

$$\varphi(t+1,x) \approx \varphi(t,x) + \partial_t \varphi(t,x) = \varphi(t,x) + v(t,x).$$

Rewriting (24) as

 $I(t,x) \approx I(t+1, x+v(t,x))$ 

and utilizing the first-order Taylor approximation of I(t + 1, x + v(t, x)) around the estimated velocity  $x + \tilde{v}(t, x)$  gives

$$I(t,x) \approx I(t+1, x + \tilde{v}(t,x)) - \nabla I(t+1, x + \tilde{v}(t,x))^{\mathrm{T}}(\tilde{v}(t,x) - v(t,x)).$$

Hence, we have

$$\widetilde{G}_{v}(t,x) \coloneqq \widetilde{\partial_{t}I(t,x)} + \widetilde{\nabla I(t,x)}^{\mathrm{T}}v(t,x) \approx 0,$$

where

$$\nabla I(t,x) \coloneqq \nabla I(t+1,x+\tilde{v}(t,x)),$$
  
$$\partial_{t}\widetilde{I(t,x)} \coloneqq I(t+1,x+\tilde{v}(t,x)) - I(t,x) - \widetilde{\nabla I(t,x)}^{\mathrm{T}}\tilde{v}(t,x).$$

We use  $\widetilde{G}_v$  to approximate the data fidelity term. Since  $\widetilde{G}_v$  requires the evaluation of I or its derivatives at points  $x + \tilde{v}(t, x)$ , which might not be on the pixel grid  $\Gamma$ , we use a bicubic interpolation.

### 5. Numerical Results

In this section, we provide a synthetic and a real-world example to demonstrate the performance of our three models and compare them with two optical flow algorithms created for general velocity fields, which do not need to be harmonic. In particular, we compare the following algorithms:

- Model I, see Theorem 4,
- Model II, see Theorem 8,
- Model III, see Theorem 9,
- the implementation of the classical Horn–Schunck method, cf. Appendix B, available in Matlab's Image Processing Toolbox, and
- the primal-dual hybrid gradient method (PDHGM) for optical flow from [2] with an  $L_1$  data fidelity term and an isotropic total variation regularizer akin to Model II.

The latter two algorithms compute the velocity  $v(t, \cdot)$  between *consecutive pairs of images*  $I(t, \cdot)$  and  $I(t + 1 \mod T, \cdot), t \in [T]$ . As the resulting  $v(t, \cdot)$  may not be of the form (7), the corresponding amplitude a is retrieved via the Fourier transform  $a(x) = 2\mathcal{F}[v](\omega, x)$ .

All numerical computations were performed on an 8-core Intel Core i7-10700 with 32 GB memory running Matlab R2022a. The code for our numerical experiments is available at [41].

#### 5.1. Generation of synthetic data

Before we come to the reconstruction in the next section, we describe how to generate the synthetic data: given a velocity field  $v: [0, T] \times \Omega \to \mathbb{R}$  and an initial image  $I_0: \Omega \to \mathbb{R}$ , we compute a sequence of distorted images I(t, x) satisfying (4). Assume that  $\varphi$  possesses an inverse function  $\psi: [0, T] \times \Omega \to \Omega$  such that

$$\varphi(t,\psi(t,x)) = x \qquad \forall (t,x) \in [0,T] \times \Omega.$$
(27)

Substituting x by  $\psi(t, x)$  in (1), we obtain

$$I(t,x) = I_0(\psi(t,x)).$$
 (28)

Thus, it remains to compute  $\psi(t, x)$ . Differentiating (27) for t, we have

$$0 = \frac{\mathrm{d}}{\mathrm{d}t}\varphi(t,\psi(t,x)) = \partial_t\varphi(t,\psi(t,x)) + \nabla\varphi(t,\psi(t,x))\partial_t\psi(t,x)$$
$$= v(t,x) + \nabla\varphi(t,\psi(t,x))\partial_t\psi(t,x),$$

where the Jacobian matrix is denoted by  $\nabla \varphi(x) = \left[\partial_{x_j} \varphi_i\right]_{i,j=1}^d$ . Differentiating (27) for x, we have

$$\nabla x = \mathrm{Id}_{d \times d} = \nabla \varphi(t, \psi(t, x)) \nabla \psi(t, x)$$

Hence, we obtain the initial value problem

$$\partial_t \psi(t, x) = -\nabla \psi(t, x) v(t, x).$$

with  $\psi(0, x) = x$ . Each component of the last equation is equivalent to the optical flow equation (3), but with different initial values in each component. For the numerical computation with the forward Euler method, we usually need to smoothen the gradient.

#### 5.2. Synthetic example

In the first experiment, we test the reconstruction algorithms on a synthetic dataset. Let  $n_1 = 200$ ,  $n_2 = 206$ , T = 300 and consider the time-harmonic velocity field v with frequency  $\omega = 6\pi/T$  and the complex amplitude  $a: \Omega \to \mathbb{C}^2$  given by

$$a(x) = \begin{bmatrix} 0.8(x_1 - \frac{n_1}{2})\sin(\frac{\|x - x_0\|^2}{2000})\exp(-\frac{\|x - x_0\|^2}{3300})\\ 10\exp(-\frac{\|x - 0.5x_0\|^2}{1650}) \end{bmatrix}, \text{ with } x_0 = \frac{1}{2} \begin{bmatrix} n_1\\ n_2 \end{bmatrix},$$

which is depicted in Figure 5 (a) and (b). From a, we compute v via (7) and turn to the simulation of the synthetic frame sequence. As an initial, undistorted image  $I_0$  depicted in Figure 5 (c), we take the resized first frame of the ultrasound gel dataset [17], which we will use in Section 5.3.



Figure 5: (a), (b): Absolute values of the two components of the ground truth amplitude  $\boldsymbol{a}$ , (c): noiseless initial image  $I_0$ , (d): initial image  $I_0$  corrupted by Poisson and salt-and-pepper noise.

We generate the frame sequence  $I = [I_0(\psi(t, x))]_{t \in [T], x \in \Gamma} \in \mathbb{R}^{T \times n_1 \times n_2}$  as described in Section 5.1, where we evaluate  $I_0$  at non-integer points or points outside the image boundary with a spline interpolation and nearest neighbor extrapolation.

Next, the vector-valued function  $a: \Omega \to \mathbb{C}^2$  is evaluated for points in  $\Gamma = [n_1] \times [n_2]$ and stored as the volume  $a \in \mathbb{C}^{2 \times n_1 \times n_2}$ . We will refer to its dimensional components  $\{a_{j,x_1,x_2}\}_{(x_1,x_2)\in\Gamma}$  as  $a_j \in \mathbb{C}^{n_1 \times n_2}$  for j = 1, 2. For the reconstruction of a from the generated images I, the algorithms are executed with the following parameters. Model I uses a coarse-to-fine pyramid with 2 levels and downsampling factor  $\eta = 0.8$ , where for each level 50 CG iterations are performed. Models II and III use 4 levels instead. Model II performs 100 CG iterations per IRLS iteration and 5 IRLS iterations (per pyramid level), while Model III performs 25 and 4 iterations, respectively. Matlab's Horn–Schunck does not use the coarse-to-fine approach and performs 1000 Horn–Schunck iterations per pair of images. PDHGM uses 15 pyramid levels with a downsampling ratio  $\eta = 0.95$ and 50 iterations per level, which are the parameters used in [2]. The regularization parameters are chosen by hand in order to receive a good result and are reported in the corresponding figures. We chose the mentioned numbers of iterations in a way such that more iterations yield only marginal improvements of the reconstructed images.

To measure the quality of reconstruction, the following metrics are considered. The relative error (RE) and relative image error (RIE) are given by

$$\operatorname{RE}(\tilde{\boldsymbol{a}}, \boldsymbol{a}) \coloneqq \frac{\sum_{j=1}^{2} \|\tilde{\boldsymbol{a}}_{j} - \boldsymbol{a}_{j}\|^{2}}{\sum_{j=1}^{2} \|\boldsymbol{a}_{j}\|^{2}} \quad \text{and} \quad \operatorname{RIE}(\tilde{\boldsymbol{I}}, \boldsymbol{I}) \coloneqq \frac{\sum_{t=1}^{T} \|\tilde{I}(t, \cdot) - I(t, \cdot)\|^{2}}{\sum_{t=1}^{T} \|I(t, \cdot)\|^{2}}$$

where  $\|\cdot\|$  is the Euclidean norm on  $\mathbb{C}^{n_1 \times n_2}$ ,  $\tilde{\boldsymbol{a}}$  is the reconstructed amplitude, and  $\tilde{\boldsymbol{I}}$  is obtained via (28) by applying to  $I_0$  the time-harmonic displacement corresponding to  $\tilde{\boldsymbol{a}}$ . Note that the RE can be seen as an analog to the end-point error used in optical flow [37]. We also report the structural similarity index measure (SSIM) [44] computed for the four frames  $\operatorname{Re}(\boldsymbol{a}_1)$ ,  $\operatorname{Im}(\boldsymbol{a}_1)$ ,  $\operatorname{Re}(\boldsymbol{a}_2)$ , and  $\operatorname{Im}(\boldsymbol{a}_2)$  with Matlab's ssim. The structural similarity index measure between the image sequences  $\boldsymbol{I}$  and  $\tilde{\boldsymbol{I}}$  is denoted by ISSIM. In our first test, we perform the reconstructions from the generated image sequence I without noise. The two spatial components  $a_j$  of the reconstructed vector field a are shown in Figure 6. We see that all compared models yield reasonable results. While Model I and the reference implementation of Matlab's Horn–Schunck yield a slightly better RE, Models II and III give a better SSIM. The error measurements for the PDHGM are in a similar magnitude, but visually the second component  $a_2$  does not completely depict the structure of the ground truth.



Figure 6: Absolute values of the spatial components  $a_j \in \mathbb{C}^{n_1 \times n_2}$  of the reconstructed amplitude  $a = (a_1, a_2)$  from the noiseless measurements smoothed with Gaussian kernel.

For our second test, the simulated images I are artificially corrupted by noise in two steps: first with the Poisson noise

$$\boldsymbol{I}_{\text{Poisson}}(t, x) = \text{Poisson}(\boldsymbol{I}(t, x)), \text{ for all } x \in \Gamma, t \in [T],$$

where Poisson denotes a Poisson random variable with parameter I(t, x). Additionally, 0.5% of the pixels in  $I_{\text{Poisson}}$  are corrupted by salt-and-pepper noise. That is, 61800 pixels (t, x) are selected randomly amongst the  $n_1n_2T$  pixels, and half of them are set to  $I_{\text{noisy}}(t, x) = 264$ , the maximal value of  $I_{\text{Poisson}}$ , and the other half of the selected pixels is set to zero. The resulting noisy image sequence is denoted by  $I_{\text{noisy}}$  and the corresponding relative error  $\text{RIE}(I_{\text{noisy}}, I)$  is 0.012. The first frame of  $I_{\text{noisy}}$  is shown in Figure 5 (d). The algorithmic setup for the noisy data is the same as before.

The reconstructions performed on the noisy images  $I_{\text{noisy}}$  are shown in Figure 7. Due to the heavy-tailed noise, Models II and III perform best in this case, while also Model I and Matlab's Horn–Schunck yield decent results. The PDHGM algorithm performs considerably worse, its implementation seems to be very reliant on a good choice of the internal parameters in case of this noisy data. Overall, the RIE must always be above a certain level due to the salt and pepper noise. Note that we compute here the RIE between the noisy images  $I_{\text{noisy}}$  and the images  $\tilde{I}$  obtained via (28) with  $I_{\text{noisy}}(0, \cdot)$  and velocity corresponding to the reconstructed amplitude  $\tilde{a}$ . Considering computational times, Model I is the fastest. Models II and III take somewhat more time, since they have an outer IRLS loop and an inner CG loop, but the inner one requires fewer iterations than Model I since it is restarted with the previous solution. The Matlab algorithm is much slower since it solves a  $2n_1n_2 \times 2n_1n_2$  linear system for each time step t, whereas Model I solves only one  $4n_1n_2 \times 4n_1n_2$  linear system to compute **a**.

#### 5.3. Real-world data

#### 5.3.1. Gel dataset

Now, we turn to the reconstruction from the real-world gel dataset, which has the size  $(n_1, n_2) = (992, 1024)$  and consists of T = 24 frames stemming from 3 oscillation periods with 8 frames each. The first frame is depicted in Figure 5 (c). It was obtained by observing a phantom specimen consisting of ultrasound gel mixed with Silicon carbide scatterers. The motion was induced by targeted sound waves with a frequency of 800 Hz perpendicular to the image plane, generated via a piezo actuator and amplifier. The resulting vibrations are recorded by a high-speed camera with a pixel size of  $2 \times 2 \,\mu\text{m}$ . More details on the measurements are found in [17].

For Model I, we perform 500 CG iterations without the coarse-to-fine pyramid. Models II and III incorporate the coarse-to-fine pyramid with 5 levels and downsampling factor  $\eta = 0.5$ . Model II performs 300 CG and 5 IRLS iterations, and Model III executes 50 CG and 6 IRLS iterations. Matlab does not use coarse-to-fine approach and performs 1000 iterations of the Horn–Schunck algorithm per pair of images. PDHGM uses the same parameters as in Section 5.2 above.



Figure 7: Absolute values of the spatial components of the reconstructed amplitude  $a = (a_1, a_2)$  from the noisy measurements  $I_n$  smoothed with Gaussian kernel.



Figure 8: Absolute values of the spatial components of the reconstructed amplitude  $a = (a_1, a_2)$  from the gel dataset.

The reconstructions are shown in Figure 8. We observe again that the accuracy of Model I and Matlab almost matches. As only T = 24 images are used, the speed benefit of Model I is less pronounced but still present. Model III is slightly faster than Model I as it uses the coarse-to-fine pyramid and performs fewer iterations on the larger images. Model II shows similar performance metrics while being slower than Model III. While the structural differences of  $\boldsymbol{a}$  are visible, this has only a minor impact on both RIE and ISSIM. The reconstruction with Model III is more consistent with the physically expected result for the homogeneous medium as it does not show such high peaks as the other models. As with the noisy simulated data, the PDHGM yields an inferior result. The first frames of the reconstructed velocity  $\boldsymbol{v}$  are plotted in Figure 9. Furthermore, we provide videos of the velocity  $\boldsymbol{v}$  and the images  $\tilde{\boldsymbol{I}}$  in the supplementary material.

#### 5.3.2. Biofilm dataset

As a non-homogeneous object to test our algorithms with, we consider a biofilm of wild-type *Bacillus subtilis* (strain NCIB361O) depicted in Figure 10. The bacteria were grown for 48 h on a substrate with 3% agar, for more details on the dataset we refer the readers to [17]. In contrast to the previous sample, the biofilm is very thin, and the central core region behaves differently from the periphery under the generated waves, which travel in the image plane. This dataset consists of T = 24 image frames with the size  $(n_1, n_2) = (992, 1024)$ . For Model I, we perform 100 CG iterations without the coarse-to-fine pyramid. Models II and III incorporate the coarse-to-fine pyramid with 5 levels and downsampling factor  $\eta = 0.5$ . Model II performs 200 CG and 10 IRLS iterations, and Model III executes 50 CG and 6 IRLS iterations. We choose the regularization parameter  $\lambda$  via a grid search to maximize the ISSIM.

The reconstructions are shown in Figure 11. All models are able to show that the central part has significantly less movement than the outer ring. While the quality metrics are in



Figure 9: Velocity maps  $||v(x,t)||_2$  corresponding to the reconstructed amplitude  $\boldsymbol{a}$ , see Figure 8, for the gel dataset and the time steps  $t = 0, \ldots, 5$  (from left to right).

a similar range for all reconstructions, there are some significant differences in the visual appearance. Models I and III yield similar-looking reconstructions. Model II produces reconstructions that look more smoothed out due to the TV-regularization. Unlike in the previous dataset, the PDHGM works comparably well with the measured reconstruction quality being on a similar level to Models I and III, but it takes considerably more time. Matlab's reconstruction gives a smaller displacement over most parts of the image, but the error measures are more comparable to Model I, similar to the other datasets. Note that the regions around the four corners are only background, so the reconstruction there is not relevant.

### 6. Conclusion

We have proposed three models for estimating the optical flow of time-harmonic oscillations. For each of them, we have derived a fast algorithm taking advantage of the single-frequency representation of the underlying displacement velocity. The conducted numerical studies suggest that Model I is the best choice for low-noise scenarios, while Model III, which combines an  $L_1$  data fidelity term with an  $L_2$  smoothness term of the gradient, performs best in the presence of heavy noise.



Figure 10: Biofilm sample  $I(0, \cdot)$ . Left: full image. Right: cut-out at center.



Figure 11: Absolute values of the spatial components of the reconstructed amplitude  $a = (a_1, a_2)$  from the biofilm dataset.

The next natural step in optical time-harmonic elastography consists of using our obtained velocity estimation for the reconstruction of the shear modulus of the examined material, see [27] or [22, § 5]. This allows us to infer information about elasticity and viscosity of observed specimen with applications to medical imaging.

#### Acknowledgements

This research was funded in whole or in part by the German Research Foundation (DFG): STE 571/19-1, project number 495365311, within the Austrian Science Fund (FWF) SFB 10.55776/F68 "Tomography Across the Scales". G.S. and I.S. acknowledge funding from the German Research Foundation (DFG) within the project BIOQIC (GRK2260). I.S. acknowledges funding by German Research Foundation (DFG) within the projects FOR5628, CRC1340 and 460333672 CRC1540 EBM. Further, this study has partially been funded by the Federal Ministry of Education and Research (BMBF, grant number 13N15754).

For open access purposes, the authors have applied a CC BY public copyright license to any author-accepted manuscript version arising from this submission.

# References

- [1] G. Aubert, R. Deriche, and P. Kornprobst. "Computing optical flow via variational techniques". SIAM Journal on Applied Mathematics 60.1 (1999), pp. 156–182.
- [2] F. Balle, T. Beck, D. Eifler, J. H. Fitschen, S. Schuff, and G. Steidl. "Strain analysis by a total generalized variation regularized optical flow model". *Inverse Problems in Science and Engineering* 27.4 (2019), pp. 540–564. DOI: 10.1080/17415977.2018.1475479.
- [3] R. Barrett, M. Berry, T. F. Chan, J. Demmel, J. Donato, J. Dongarra, V. Eijkhout, R. Pozo, C. Romine, and H. Van der Vorst. *Templates for the solution of linear systems: building blocks for iterative methods.* SIAM, 1994.
- [4] J. L. Barron, D. J. Fleet, and S. S. Beauchemin. "Performance of optical flow techniques". International Journal of Computer Vision 12.1 (1994), pp. 43–77. DOI: 10.1007/bf01420984.
- [5] A. Beck. First-Order Methods in Optimization. SIAM, 2017.
- [6] F. Becker, S. Petra, and C. Schnörr. "Optical flow". In: Handbook of Mathematical Methods in Imaging. New York: Springer, 2015, pp. 1945–2004. DOI: 10.1007/978-1-4939-0790-8\_38.
- [7] R. Bergmann, R. Chan, R. Hielscher, J. Persch, and G. Steidl. "Restoration of manifold-valued images by half-quadratic minimization". *Inverse Problems and Imaging* 10.2 (2016), pp. 281–304.
   DOI: 10.3934/ipi.2016001.
- [8] P. Bloomfield and W. L. Steiger. Least Absolute Deviations. Birkhäuser Boston, 1984. DOI: 10. 1007/978-1-4684-8574-5.
- [9] T. Brox, A. Bruhn, N. Papenberg, and J. Weickert. "High accuracy optical flow estimation based on a theory for warping". In: *Computer Vision - ECCV 2004.* Springer Berlin Heidelberg, 2004, pp. 25–36. DOI: 10.1007/978-3-540-24673-2\_3.
- P. Flotho, C. Heiss, G. Steidl, and D. Strauss. "Lagrangian motion magnification with double sparse optical flow decomposition". *Frontiers in Applied Mathematics and Statistics* 9 (2023), p. 1164491. DOI: 10.3389/fams.2023.1164491.
- [11] D. Fortun, P. Bouthemy, and C. Kervrann. "Optical flow modeling and computation: a survey". Computer Vision and Image Understanding 134 (2015). DOI: 10.1016/j.cviu.2015.02.008.
- [12] B. Goldluecke and D. Cremers. "An approach to vectorial total variation based on geometric measure theory". In: 2010 IEEE Computer Society Conference on Computer Vision and Pattern Recognition. IEEE, 2010. DOI: 10.1109/CVPR.2010.5540194.
- [13] M. Gräf, S. Neumayer, R. Hielscher, G. Steidl, M. Liesegang, and T. Beck. "An image registration model in electron backscatter diffraction". SIAM Journal on Imaging Sciences 15.1 (2022), pp. 228–260. DOI: 10.1137/21M1426353.
- [14] W. Hinterberger, O. Scherzer, C. Schnörr, and J. Weickert. "Analysis of optical flow models in the framework of calculus of variations". *Numerical Functional Analysis and Optimization* 23.1/2 (2002), pp. 69–89.
- B. K. Horn and B. G. Schunck. "Determining optical flow". Artificial Intelligence 17.1-3 (1981), pp. 185–203. DOI: 10.1016/0004-3702(81)90024-2.
- [16] Z. Huang. Awesome Optical Flow. 2024. URL: https://github.com/hzwer/Awesome-Optical-Flow/tree/b3aff0d34ecfb1e7243bbb8f62f7d6732e7e7e20.
- [17] J. Jordan, N. Jaitner, T. Meyer, L. Brahmè, M. Ghrayeb, J. Köppke, S. K. Chandia, V. Zaburdaev, L. Chai, H. Tzschätzsch, J. Mura, A. I. Hagemann, J. Braun, and I. Sack. "Optical time-harmonic elastography for multiscale stiffness mapping across the phylogenetic tree". *Advanced Sciences* (in print). DOI: 10.1002/advs.202410473.

- [18] L. Krainz, E. Sherina, S. Hubmer, M. Liu, W. Drexler, and O. Scherzer. "Quantitative optical coherence elastography: a novel intensity-based inversion method versus strain-based reconstructions". *IEEE Journal of Selected Topics in Quantum Electronics* 29.4: Biophotonics (2022), pp. 1– 16. DOI: 10.1109/jstqe.2022.3225108.
- [19] C. Kümmerle, C. Mayrink Verdun, and D. Stöger. "Iteratively reweighted least squares for basis pursuit with global linear convergence rate". In: *NeurIPS*. 2021.
- [20] L. Li and Y. Yang. "Optical flow estimation for a periodic image sequence". IEEE Transactions on Image Processing 19.1 (2010), pp. 1–10. DOI: 10.1109/tip.2009.2032341.
- [21] B. Lucas and T. Kanade. "An iterative image registration technique with an application to stereo vision". In: International Joint Conference on Artificial Intelligence. 1981, pp. 674–679.
- [22] A. Manduca, T. Oliphant, M. Dresner, J. Mahowald, S. Kruse, E. Amromin, J. Felmlee, J. Greenleaf, and R. Ehman. "Magnetic resonance elastography: non-invasive mapping of tissue elasticity". *Medical Image Analysis* 5.4 (2001), pp. 237–254. DOI: 10.1016/s1361-8415(00) 00039-6.
- [23] C. Mayrink Verdun, O. Melnyk, F. Krahmer, and P. Jung. "Fast, blind, and accurate: tuning-free sparse regression with global linear convergence". In: *Proceedings of Thirty Seventh Conference* on Learning Theory. Ed. by S. Agrawal and A. Roth. Vol. 247. Proceedings of Machine Learning Research. PMLR, 2024, pp. 3823–3872. URL: https://proceedings.mlr.press/v247/mayrinkverdun24a.html.
- [24] T. Meyer, J. Castelein, J. Schattenfroh, A. S. Morr, R. Vieira da Silva, H. Tzschätzsch, R. Reiter, J. Guo, and I. Sack. "Magnetic resonance elastography in a nutshell: tomographic imaging of soft tissue viscoelasticity for detecting and staging disease with a focus on inflammation". Progress in Nuclear Magnetic Resonance Spectroscopy 144-145 (2024), pp. 1–14. DOI: 10.1016/j.pnmrs. 2024.05.002.
- [25] J. Modersitzki. FAIR: Flexible Algorithms for Image Registration. Philadelphia: SIAM, 2009.
- [26] J. Modersitzki. Numerical Methods for Image Registration. New York: Oxford University Press, 2003. ISBN: 978-0198528418. DOI: 10.1093/acprof:oso/9780198528418.001.0001.
- [27] S. Papazoglou, S. Hirsch, J. Braun, and I. Sack. "Multifrequency inversion in magnetic resonance elastography". *Physics in Medicine and Biology* 57.8 (2012), pp. 2329–2346. DOI: 10.1088/0031– 9155/57/8/2329.
- [28] W. Qi, X. Niu, and Y. Yang. "An improved periodic optical flow model for cardiac gated image reconstruction". In: 2011 IEEE International Symposium on Biomedical Imaging: From Nano to Macro. IEEE. 2011, pp. 1276–1279. DOI: 10.1109/ISBI.2011.5872634.
- [29] J. Revell, M. Mirmehdi, and D. McNally. "Computer vision elastography: speckle adaptive motion estimation for elastography using ultrasound sequences". *IEEE Transactions on Medical Imaging* 24.6 (2005), pp. 755–766. DOI: 10.1109/tmi.2005.848331.
- [30] L. Rudin, S. Osher, and E. Fatemi. "Nonlinear total variation based noise removal algorithms". *Physica D: Nonlinear Phenomena* 60.1 (1992), pp. 259–268. DOI: 10.1016/0167-2789(92)90242-F.
- [31] I. Sack. "Magnetic resonance elastography from fundamental soft-tissue mechanics to diagnostic imaging". *Nature Reviews Physics* 5.1 (2023), pp. 25–42. DOI: 10.1038/s42254-022-00543-2.
- [32] J. Schmitt. "OCTelastography: imaging microscopic deformation and strain of tissue". Opt Express 3.6 (1998), pp. 199–211. DOI: 10.1364/oe.3.000199.
- [33] S. Shah and X. Xuezhi. "Traditional and modern strategies for optical flow: an investigation". SN Applied Sciences 3.289 (2021). DOI: 10.1007/s42452-021-04227-x.

- [34] E. Sherina, L. Krainz, S. Hubmer, W. Drexler, and O. Scherzer. "Challenges for optical flow estimates in elastography". In: Scale Space and Variational Methods in Computer Vision. SSVM 2021. 2021, pp. 128–139. DOI: 10.1007/978-3-030-75549-2\_11.
- [35] E. Sherina, L. Krainz, S. Hubmer, W. Drexler, and O. Scherzer. "Displacement field estimation from OCT images utilizing speckle information with applications in quantitative elastography". *Inverse Problems* 36.12 (2020), p. 124003. DOI: 10.1088/1361-6420/abaf65.
- [36] X. Shi, Z. Huang, W. Bian, D. Li, M. Zhang, K. C. Cheung, S. See, H. Qin, J. Dai, and H. Li. "Videoflow: exploiting temporal cues for multi-frame optical flow estimation". In: *Proceedings of the IEEE/CVF International Conference on Computer Vision*. 2023, pp. 12469–12480.
- [37] D. Sun, S. Roth, and M. Black. "A quantitative analysis of current practices in optical flow estimation and the principles behind them". *International Journal on Computer Vision* 106 (2014), pp. 115–137. DOI: 10.1007/s11263-013-0644-x.
- [38] D. Sun, S. Roth, and M. Black. "Secrets of optical flow estimation and their principles". In: 1010 IEEE Computer Society Conference on Computer Vision and Pattern Recognition. 2010, pp. 2432–2439. DOI: 10.1109/CVPR.2010.5539939.
- [39] Z. Teed and J. Deng. "RAFT: recurrent all-pairs field transforms for optical flow". In: ECCV. Springer. 2020, pp. 402–419.
- [40] A. K. Z. Tehrani, M. Mirzaei, and H. Rivaz. "Semi-supervised training of optical flow convolutional neural networks in ultrasound elastography". In: *Medical Image Computing and Computer* Assisted Intervention – MICCAI 2020. Cham: Springer, 2020, pp. 504–513.
- [41] Time-Harmonic Elastography repository on Github. URL: https://github.com/Sniper2k/Time-Harmonic-Elastography.
- [42] H. Tzschätzsch, T. Elgeti, K. Rettig, C. Kargel, R. Klaua, M. Schultz, J. Braun, and I. Sack. "In vivo time harmonic elastography of the human heart". Ultrasound in Medicine & Biology 38.2 (2012), pp. 214–222. DOI: 10.1016/j.ultrasmedbio.2011.11.002.
- [43] Q. Wang, Y.-Y. Chang, R. Cai, Z. Li, B. Hariharan, A. Holynski, and N. Snavely. "Tracking everything everywhere all at once". *ArXiv:2306.05422* (2023).
- [44] Z. Wang, A. C. Bovik, H. R. Sheikh, and E. P. Simoncelli. "Image quality assessment: from error visibility to structural similarity". *IEEE Transaction on Image Processing* 13 (2004), pp. 600– 612. DOI: 10.1109/TIP.2003.819861.
- [45] J. Weickert, A. Bruhn, T. Brox, and N. Papenberg. "A survey on variational optic flow methods for small displacements". In: *Mathematical Models for Registration and Applications to Medical Imaging*. Ed. by O. Scherzer. Berlin, Heidelberg: Springer, 2006, pp. 103–136. DOI: 10.1007/978– 3-540-34767-5\_5.
- [46] J. Weickert and C. Schnörr. "Variational optic flow computation with a spatio-temporal smoothness constraint". Journal of Mathematical Imaging and Vision 14.3 (2001), pp. 245–255. DOI: 10.1023/a:1011286029287.
- [47] W. Wirtinger. "Zur formalen Theorie der Funktionen von mehr komplexen Veränderlichen". Mathematische Annalen 97.1 (1927), pp. 357–375. DOI: 10.1007/BF01447872.
- [48] M. Zhai, X. Xiang, N. Lv, and X. Kong. "Optical flow and scene flow estimation: a survey". Pattern Recognition 114 (2021), p. 107861. DOI: 10.1016/j.patcog.2021.107861.
- [49] F. Zvietcovich, P. Pongchalee, P. Meemon, J. P. Rolland, and K. J. Parker. "Reverberant 3D optical coherence elastography maps the elasticity of individual corneal layers". *Nature Communications* 10.1 (2019), p. 4895. DOI: 10.1038/s41467-019-12803-4.

### A. Periodicity of u versus v

We look at another one-dimensional example where the displacement u can be described by a single harmonic, namely

$$\varphi(t,x) = x + c(1-x^2)\sin(t), \qquad x \in [-1,1], \ t \ge 0,$$
(29)

with some c > 0, see Figure 12 left. Denoting again by  $\psi$  the inverse of  $\varphi$  as in (27), we get

$$x = \psi(t, y) = \frac{1 - \sqrt{4c^2 \sin^2(t) - 4cy \sin(t) + 1}}{2c \sin(t)}$$

and the velocity

$$v(t,y) = \partial_t \varphi(t,\psi(t,y)) = c(\psi(t,y)^2 - 1)\cos(t)$$
  
=  $\cos(t) \frac{\sqrt{4c^2 \sin^2(t) - 4cy \sin(t) + 1} + 2cy \sin(t) - 1}{2c \sin^2(t)}$ 

see Figure 12 right. The flow velocity  $v(t, \psi(t, y))$  is still  $2\pi$ -periodic in t, but it is not a single harmonic anymore.



Figure 12: Trajectories  $\varphi(t, x)$  (left) and flow velocity v(t, x) (right) corresponding to (29) for different values of x and fixed c = 0.1 and  $\omega = 1$ .

## B. The classical Horn–Schunck algorithm

The classical Horn–Schunck algorithm as proposed in [15] can be straightforwardly adopted to solve (13) in the following way. We again split up real and imaginary part,

as the complex equation contains both a and its conjugate  $\overline{a}$ . Then, in matrix form, (13) reads as

$$\lambda T \begin{pmatrix} \Delta a_{\mathrm{R}}(x) \\ \Delta a_{\mathrm{I}}(x) \end{pmatrix} = C(x) \begin{pmatrix} a_{\mathrm{R}}(x) \\ a_{\mathrm{I}}(x) \end{pmatrix} + 2 \begin{pmatrix} \mathrm{Re}\mathcal{F}[\partial_{t}I\nabla_{x}I^{\mathrm{T}}](\omega, x) \\ \mathrm{Im}\mathcal{F}[\partial_{t}I\nabla_{x}I^{\mathrm{T}}](\omega, x) \end{pmatrix}$$

with the coefficient matrix

$$C(x) = \begin{pmatrix} \operatorname{Re}\mathcal{F}[\nabla_x I \nabla_x I^{\mathrm{T}}](2\omega, x) & \operatorname{Im}\mathcal{F}[\nabla_x I \nabla_x I^{\mathrm{T}}](2\omega, x) \\ \operatorname{Im}\mathcal{F}[\nabla_x I \nabla_x I^{\mathrm{T}}](2\omega, x) & -\operatorname{Re}\mathcal{F}[\nabla_x I \nabla_x I^{\mathrm{T}}](2\omega, x) \end{pmatrix} + I_2 \otimes \mathcal{F}[\nabla_x I \nabla_x I^{\mathrm{T}}](x, 0),$$

where  $\otimes$  is the Kronecker product and  $I_2$  is the 2 × 2 identity matrix. By rewriting the system as

$$\lambda T \begin{pmatrix} (\Delta - 1)a_{\mathrm{R}}(x) \\ (\Delta - 1)a_{\mathrm{I}}(x) \end{pmatrix} = \left[ C(x) + \lambda T \operatorname{I}_{2d} \right] \begin{pmatrix} a_{\mathrm{R}}(x) \\ a_{\mathrm{I}}(x) \end{pmatrix} + 2 \begin{pmatrix} \operatorname{Re}\mathcal{F}[\partial_{t}I\nabla_{x}I^{\mathrm{T}}](\omega, x) \\ \operatorname{Im}\mathcal{F}[\partial_{t}I\nabla_{x}I^{\mathrm{T}}](\omega, x) \end{pmatrix},$$

the right-hand side depends only on  $a_{\rm R}$  and  $a_{\rm I}$  evaluated at a single point x. If the left-hand side were independent of the values of a at points other than x, we could significantly simplify the computational effort and solve a separate linear system for each x. However, the Laplacian requires the values of  $a_{\rm R}$  and  $a_{\rm I}$  in a neighborhood of x. To avoid a large linear system, one solves (13) with the following iterative procedure. Starting with initial  $a_{\rm R}^0$  and  $a_{\rm I}^0$ , we construct for  $k \ge 0$  new iterates  $a_{\rm R}^{k+1}$  and  $a_{\rm I}^{k+1}$  by solving for each x the  $2d \times 2d$  linear system

$$\lambda T \begin{pmatrix} (\Delta - 1)a_{\mathrm{R}}^{k}(x) \\ (\Delta - 1)a_{\mathrm{I}}^{k}(x) \end{pmatrix} = \left[ C(x) + \lambda T \operatorname{I}_{2d} \right] \begin{pmatrix} a_{\mathrm{R}}^{k+1}(x) \\ a_{\mathrm{R}}^{k+1}(x) \end{pmatrix} + 2 \begin{pmatrix} \operatorname{Re}\mathcal{F}[\partial_{t}I\nabla_{x}I^{\mathrm{T}}](\omega, x) \\ \operatorname{Im}\mathcal{F}[\partial_{t}I\nabla_{x}I^{\mathrm{T}}](\omega, x) \end{pmatrix}$$

When discretizing a on a uniform grid,  $(\Delta - 1)a(x)$  is implemented as the mean value over the grid points adjacent to x.

### C. Construction of the linear system for Model I

In this section, we consider the discretization of (13) in a one-dimensional setting. Let  $d = 1, n_1 = n$  and assume that  $T = 2p\pi/\omega \in \mathbb{N}$  for some  $p \in \mathbb{N}$ . While it is possible to directly replace the operators in (13) with their discrete analogues, we first go a step back and start with the minimization of the energy functional E for Model I. Its empirical counterpart  $E_{\text{emp}} \colon \mathbb{C}^n \to \mathbb{R}$  for observed images  $\mathbf{I} \in \mathbb{R}^{T \times n}$  is given by

$$E_{\rm emp}(\boldsymbol{a}) = \sum_{x \in \Gamma} \sum_{t=0}^{T-1} \left( \left( \boldsymbol{D}_c \boldsymbol{I}(t, x)^{\top} \boldsymbol{a}_{\rm R}(x) \cos(t\omega) + \boldsymbol{D}_c \boldsymbol{I}(t, x)^{\top} \boldsymbol{a}_{\rm I}(x) \sin(-t\omega) + \boldsymbol{D}_t \boldsymbol{I}(t, x) \right)^2 + \lambda |\boldsymbol{D} \boldsymbol{a}_{\rm R}(x) \cos(t\omega) + \boldsymbol{D} \boldsymbol{a}_{\rm I}(x) \sin(-t\omega)|^2 \right),$$

where  $\Gamma = [n]$  is the pixel grid,  $D_c$  denotes the one-dimensional discrete central derivatives as in (24) and  $D, D_t$  are the forward difference operators (25) in space and time, respectively. As d = 1, we leave out the extra index for the simplicity of notation. Minimizing  $E_{\rm emp}$  can be viewed as a least squares problem. Introducing the matrices

$$oldsymbol{y} \coloneqq - egin{bmatrix} oldsymbol{D}_t oldsymbol{I}(\cdot, 0) \ dots \ oldsymbol{D}_t oldsymbol{I}(\cdot, T-1) \end{bmatrix}, \quad oldsymbol{R} \coloneqq egin{bmatrix} oldsymbol{D} & 0 \ 0 & oldsymbol{D} \end{bmatrix}, \quad oldsymbol{M} \coloneqq egin{bmatrix} oldsymbol{M}_{0,1} & oldsymbol{M}_{0,2} \ dots & dots \ oldsymbol{D}_t oldsymbol{I}(\cdot, T-1) \end{bmatrix},$$

with blocks

 $\boldsymbol{M}_{t,1} \coloneqq \operatorname{diag}(\boldsymbol{D}_c \boldsymbol{I}(t,\cdot)) \cos(-2\pi t p/T), \text{ and } \boldsymbol{M}_{t,2} \coloneqq \operatorname{diag}(\boldsymbol{D}_c \boldsymbol{I}(t,\cdot)) \sin(-2\pi t p/T),$ and simplifying the regularizer as in (14) transforms the energy functional  $E_{\text{emp}}$  into

$$E_{\rm emp}(\boldsymbol{a}) = \left\| \boldsymbol{M} \begin{bmatrix} \boldsymbol{a}_{\rm R} \\ \boldsymbol{a}_{\rm I} \end{bmatrix} - \boldsymbol{y} \right\|_{2}^{2} + \frac{\lambda T}{2} \left\| \boldsymbol{R} \begin{bmatrix} \boldsymbol{a}_{\rm R} \\ \boldsymbol{a}_{\rm I} \end{bmatrix} \right\|_{2}^{2} = \left\| \begin{bmatrix} \boldsymbol{M} \\ \sqrt{\frac{\lambda T}{2}} \boldsymbol{R} \end{bmatrix} \begin{bmatrix} \boldsymbol{a}_{\rm R} \\ \boldsymbol{a}_{\rm I} \end{bmatrix} - \begin{bmatrix} \boldsymbol{y} \\ 0 \end{bmatrix} \right\|_{2}^{2}$$

Its normal equation, which is the discrete analogue of the Euler–Lagrange equations that lead us to (13), is given by

$$\boldsymbol{C}\begin{bmatrix}\boldsymbol{a}_{\mathrm{R}}\\\boldsymbol{a}_{\mathrm{I}}\end{bmatrix} \coloneqq \left(\boldsymbol{M}^{\mathsf{T}}\boldsymbol{M} + \frac{\lambda T}{2}\boldsymbol{R}^{\mathsf{T}}\boldsymbol{R}\right)\begin{bmatrix}\boldsymbol{a}_{\mathrm{R}}\\\boldsymbol{a}_{\mathrm{I}}\end{bmatrix} = \boldsymbol{M}^{\mathsf{T}}\boldsymbol{y} \eqqcolon \boldsymbol{b}, \qquad (30)$$

which is precisely (26). Moreover, C is square, symmetric and positive semidefinite.

It remains to argue that (30) corresponds to the direct discretization of (13). For this, we observe that the matrix C and the vector b admit the block structure

$$oldsymbol{C} = egin{bmatrix} oldsymbol{C}_{1,1} & oldsymbol{C}_{1,2} \ oldsymbol{C}_{2,1} & oldsymbol{C}_{2,2} \end{bmatrix}, \quad oldsymbol{b} = egin{bmatrix} oldsymbol{b}_1 \ oldsymbol{b}_2 \end{bmatrix},$$

with

$$\begin{split} \boldsymbol{C}_{1,1} &= \sum_{t=0}^{T-1} \operatorname{diag}(\boldsymbol{D}_{c}\boldsymbol{I}(t,\cdot) \circ \boldsymbol{D}_{c}\boldsymbol{I}(t,\cdot)) \cos^{2}(-t\omega) + \frac{\lambda T}{2}\boldsymbol{D}^{\mathsf{T}}\boldsymbol{D} \\ &= \sum_{t=0}^{T-1} \operatorname{diag}(\boldsymbol{D}_{c}\boldsymbol{I}(t,\cdot) \circ \boldsymbol{D}_{c}\boldsymbol{I}(t,\cdot)) \left[\frac{1}{2} + \frac{\cos(-2\pi tp/T)}{2}\right] + \frac{\lambda T}{2}\boldsymbol{D}^{\mathsf{T}}\boldsymbol{D} \\ &= \operatorname{diag}\left(\frac{1}{2}\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I} \circ \boldsymbol{D}_{c}\boldsymbol{I}](0,\cdot) + \frac{1}{2}\operatorname{Re}\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I} \circ \boldsymbol{D}_{c}\boldsymbol{I}](2p,\cdot)\right) + \frac{\lambda T}{2}\boldsymbol{D}^{\mathsf{T}}\boldsymbol{D}, \end{split}$$

and, similarly,

$$C_{1,2} = C_{2,1} = \operatorname{diag}\left(\frac{1}{2}\operatorname{Im}\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I}\circ\boldsymbol{D}_{c}\boldsymbol{I}](2p,\cdot)\right),$$

$$C_{2,2} = \operatorname{diag}\left(\frac{1}{2}\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I}\circ\boldsymbol{D}_{c}\boldsymbol{I}](0,\cdot) - \frac{1}{2}\operatorname{Re}\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I}\circ\boldsymbol{D}_{c}\boldsymbol{I}](2p,\cdot)\right) + \frac{\lambda T}{2}\boldsymbol{D}^{\top}\boldsymbol{D},$$

$$\boldsymbol{b}_{1} = \operatorname{Re}\left(\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I}\circ\boldsymbol{D}_{t}\boldsymbol{I}](p,\cdot)\right), \qquad \boldsymbol{b}_{2} = \operatorname{Im}\left(\boldsymbol{F}[\boldsymbol{D}_{c}\boldsymbol{I}\circ\boldsymbol{D}_{t}\boldsymbol{I}](p,\cdot)\right),$$

where  $\circ$  denotes the entrywise product and  $\boldsymbol{F}$  is the discrete Fourier transform (23). Since  $\boldsymbol{D}^{\top}\boldsymbol{D}$  is a discrete approximation of the negative Laplacian  $-\Delta$ , we see that (30) is indeed a discretization of (13).